

Stability of external and internal implant connections after a fatigue test

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ABSTRACT

Objective: The objective of this study was to compare the torque and detorque values of screw intermediates of external hexagon, internal hexagon, and Morse taper implants in single restorations before and after mechanical cycling. **Materials and Methods:** The study sample was divided into three groups ($n = 10$) as follows: group EH – external hexagon implant, group IH – internal hexagon implant, and group MT – Morse taper implant. Universal abutments were screwed on the implants, and metal crowns were cemented onto the abutment. The samples were submitted to a mechanical testing of 1 million cycles, with a frequency of 8 cycles per second under a 400 N load. The application and registration of the screw torque (T0) and detorque (T1) values of the intermediate were performed before and after the test. The results were statistically evaluated by analysis of variance (ANOVA) and Tukey's test ($\alpha = 0.05$). **Results:** There was no difference between the values of T0 and T1 in the intra-group samples. However, the inter-group difference in T0 between the EH (12.8 N cm) and MT (18.6 N cm) groups and in T1 between the EH (10.4 N cm) and IH (13.8 N cm), EH and MT (19.4 N cm), and MT and IH ($P = 0.001$) groups were significant. The MT group showed a lower variation of T0 and T1. **Conclusion:** The internal implants, particularly MT, showed better stability in these cases when used for single restorations.

Key words: Dental implant, dental prosthesis, dental prosthesis retention, fatigue

INTRODUCTION

Dental rehabilitation via implant support has become a routine procedure. In many cases, this is the first option for dentists who are deliberating treatment plans. Implants are an alternative not only for the treatment of total edentulism but also for the replacement of one or more dental elements.^[1] The careful consideration of technical parameters and biomechanical parameters, in addition to aesthetic requirements, is imperative.^[2]

Several studies have been conducted with the goal of achieving an accurate and stable connection between the components of implant systems.^[1-6] The connection is achieved by means of bolts created by the union between the implant and the prosthetic component.^[1,3-5]

The most frequently observed complication of screwed and cemented prostheses is loosening of the screw that leads to a misfit of the abutment to the implant after the prosthesis is in use.^[1,3-6] The combination of horizontal and vertical misfits may result in a gap leading to an increased area of bacterial accumulation, which complicates clean-up^[7,8] and causes gingival inflammation due to the development of microflora in the gap region. Peri-implantitis and subsequent risks of bone resorption as well as posterior fracture of the screw can develop.^[9]

The screw torque determines the preload. The tensile strength is the initial reaction that generates a compressive force between the components of the prosthesis, which keeps them set together.^[2] In addition to the preload, another fundamentally

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important factor determining the stability of the implant/prosthesis complex is the conical geometric configuration of the connection between the implant and the prosthetic components of internal and external hexagon connection systems.^[1,3]

In view of the fact that one of the factors of successful maintenance of the prosthesis on the implant is the stability of single restoration screw implants, which tend to become loose after some time of use, the aim of this study was to verify, before and after a fatigue test (cyclic mechanical testing), the detorque value of the different geometric configurations of the internal hexagon, external hexagon, and Morse taper implants with simulation of a year of function.

The hypothesis of this study is that mechanical cycling and geometry of dental implants can interfere with the detorque values and Morse taper connection presents less variation between the initial and final torque.

MATERIALS AND METHODS

A total of 30 implants (of 4.3 mm diameter × 13 mm length) and prosthetic components (Neodent, Curitiba, Parana, Brazil) were distributed into three groups: Group EH (external hexagon) – Alvim Ti, group IH (internal hexagon) – Alvim II Plus, and group MT (Morse taper) – CM Alvim. The dental implants were included in an epoxy resin–glass fiber composite (NEMA Grade G-10 rod, Piedmont Plastics, Charlotte, NC, USA) using a parallelometer (Bioart, St. Charles, SP, Brazil), which ensures that the implants are parallel to each other^[10] and standardize the incidence of loading cyclic during fatigue test that was subsequently performed. This embedded material has an appropriate elastic modulus (approximately 20 GPa) similar to bone;^[11] it is easily machined and is sufficiently tough to allow cyclic testing.

To construct the coronal part, prefabricated abutments were used. For the EH and IH groups, a universal abutment anti-rotational (Tilite) with a diameter of 4.3 mm and a titanium screw (Neotorque, Neodent, Curitiba, Brazil) were used. For the MT group, the abutment, 4.3 mm in diameter, was first attached to a cemented component burnout. They were then fixed onto the implants with a manual key and fixed onto the same standardized waxed crowns, fabricated using a matrix of silicon (Poly 1 N, Polasil, São Paulo, Brazil) for each connection type, representing right mandibular second premolar. The wax maintained access to the screw so that the torque could be

recorded after the test even after the prostheses were cemented. For the casting of the crowns, Tilite alloy, composed of nickel, chromium, and titanium, was used (Talladium, Curitiba, PR, Brazil), and the casting process using lost wax (under flame) was performed according to the manufacturer's recommendations.

The access to the screw holes, the abutment, and the crown was protected with polyvinylsiloxane (Adsil/Vigodent, Rio de Janeiro, Brazil) during cementing of the crowns. For this procedure, zinc phosphate cement (SS White, Rio de Janeiro, Brazil) was used according to the specifications of the manufacturer; the crowns were cemented one by one by a single operator; they were kept in the lathe vise (SomarAdd, São Paulo, SP, Brazil) for 10 min under finger pressure. Regarding the cementation technique, the literature shows that not only the pressure used but also whether it is static or dynamic may interfere with the thickness of the film.^[12]

For the application of a torque, the samples were firmly fixed on a bench (Somar, São Paulo, Brazil). Initially, two torques of the same value (20 N cm, according to the manufacturer) were applied, with a 10-min break between them. An analog torque meter (Tohnichi BTG60CN, Tohnichi, Tokyo, Japan) was used to achieve maximum preload. After 2 min of the second torque, the value of detorque was measured and recorded according to the methodology proposed by Khraisat *et al.* in 2004.^[13] The samples underwent cyclic mechanical testing (Instron 8801, Instron, Grove City, PA, USA), whereby 400 N of axial force was applied over a crown surface at a frequency of 8 Hz for a total of 1 million cycles; this process simulated a year of implant function.^[10] After the fatigue test, the samples were set on the torque meter to measure and record the final detorque value as previously described.

The averages were calculated and statistically analyzed by two-way analysis of variance (ANOVA) and Tukey's test at a 5% significance level. The initial and final detorque values and the intra- and inter-group differences between these values were assessed.

RESULTS

Table 1 shows the data of the average initial detorque (T0) and final detorque (T1) values (N cm), with $\alpha = 0.05$.

Table 1: Descriptive data of average detorque (N cm) initial (T0) and final (T1) values

Group	T0	T1
EH	12.80±2.86 B,a	10.40±0.55 C,a
IH	15.40±2.07 AB,a	13.80±1.30 B,a
MT	18.60±0.89 A,a	19.40±0.55 A,a

Means followed by different capital letters in the same column, and small letters in the same line, were significantly different ($P < 0.05$), IH: Internal hexagon, EH: External hexagon, MT: Morse taper

There was no statistically significant difference between the values of T0 and T1 of the intra-group samples. However, a statistically significant difference in T0 was found between the EH and MT groups ($P = 0.012$). The MT group obtained higher T0 values than the EH group, and the IH group obtained intermediate values of T0 without statistical difference. The T1 means showed that the MT group obtained the highest values followed by the IH and EH groups, which had the lowest values of T1 ($P = 0.001$).

DISCUSSION

The implant/abutment interface has been reported to be the primary factor in stress distribution, adverse biological responses, and other prosthetic complications.^[3,4] Therefore, torque plays an important role in maintaining the integrity of the implant/abutment interface, as it reduces the tendency of screw loosening and margin opening when it is correctly applied with accuracy and proper technique. In a recently published systematic review on implant-related complications, Jung *et al.*^[14] calculated the cumulative incidence of connection-related complications (screw loosening, 12.7% and fracture, 0.35%) in 5 years of clinical service. Gokcen-Rohlig *et al.*^[15] found similar results.

Despite the widespread use of external hexagon connections,^[3,11,16] failure rates ranging from 6 to 48% have been described in the medical literature. A lower stability of external connections was found when the results of this study were analyzed. The initial detorque (T0) and final detorque (T1) values found in the EH group were statistically lower than those measured in the MT group and IH group when considering the values shown in T1; these results are in agreement with other studies.^[11,17]

This greater stability of the internal connections, especially the Morse taper, is important because it provides more predictable rehabilitation with greater longevity and success rates. This connection provides higher resistance at the implant/abutment interface, anti-rotational characteristics, and resistance

to loosening of the screw.^[1,16-19] Both the internal hexagon connection and the Morse taper had higher final detorque values (T1) when compared with the values of the external hexagon connection, although the difference between the values of the initial detorque (T0) of the external and internal hexagon were not statistically significant. Compared with the internal hexagon connection, torque loss was not obtained in the Morse taper connection after cyclic testing, and the difference was statistically significant. Squier *et al.* in 2002^[20] stated that abutments of the Morse taper connection showed detorque values higher than the initial torque due to the cold solder on the implant/abutment interface agreement with the results of this study. This condition arises from the friction between the two surfaces, which differ slightly; the pressure created by the insertion force determines the maintenance of the connection even after stopping the applied force for insertion.

Another factor of great importance for the stability of the connection is the screw. Its shape, size, and coating material, as well as the compressive force it exerts, known as preload, are crucial to maintaining stability of the connection; this has already been studied extensively.^[20-22] The material of the screw is the most significant factor in determining the characteristics of its union.^[3] The threads of the titanium screw, in contact with the threads of the implant, promote a connection that results from the sliding contact between the inner surfaces of the same material. This form of contact results in a greater coefficient of friction. Gold screws have a low coefficient of friction, which allows higher torque values without the threads adhering to the titanium threads of the implant. In an attempt to reduce the coefficient of friction, manufacturers surface treat the screws. In 2001, Martin *et al.*^[23] investigated the generation of preload in four brands of screws and concluded that surface treatment of bolts reduced the coefficient of friction, resulting in higher preload values. Factors that influence preload are the geometry of the screw (thread pitch) and the mechanical properties of metal, including texture, surface finishing, surface settlement, and degree of lubrication.^[5,9,16,24-27]

The screws used in this study had the same characteristics for all groups, so the difference was the contact surface and the interaction between the screw and the internal surface of the implant due to differences in implant geometries (external, internal, and Morse). The results obtained in this study agree with those of other studies in the literature^[11,28] which show that internal connections are more stable mechanically than external flat connections. The general focus is clearly

on deep internal connections in which the screw takes little or no load and provides intimate contact with the implant walls to resist micromovement.

Important issues to be addressed are the amount of torque to be applied and the device used. The literature states that the maximum torque should not exceed 75% of the maximum strength of the bolts and that the torque recommended by the manufacturer varies with the type, configuration, and diameter of the device.^[25] The device used to apply the torque in this study had an accuracy of about 98%.

Fatigue tests allow simulation of clinical function. However, published studies have used different methodologies for the applied axial load, frequency, and number of cycles.^[5,26,27] The frequency of cycles is reported in the literature as ranging from 1 to 19 Hz.^[27] It was clarified that in a day, an individual typically performs three episodes of chewing lasting 15 min, with a frequency of 60 cycles per minute (1 Hz); this generates 2700 chewing cycles per day, which equals 1 million cycles per annum.^[26] Considering that the frequency appears to have little importance in fatigue studies, the methodology uses a frequency of 8 Hz.^[10] The reported incident forces in molars ranged from 390 to 880 N, in premolars was 453 N, and in incisors was 222 N. Thus, a load of 400 N was used in the region of the premolar.^[6,10]

The results obtained after the fatigue test showed a decrease of torque in samples of the different groups. The decrease of torque was more evident in the external hexagonal connections followed by the internal hexagon connections; the best result was found in the Morse taper connections, which indicates that the initial hypothesis is true.

Finally, although laboratory studies have limitations that should be considered when compared with the clinical reality, these studies are important as they contribute to the advancement of dentistry. In this study, different internal geometries of dental implants were investigated; however, the abutments and screws used were of the same materials and geometry. Thus, future studies comparing different geometries and materials of abutment and screw should be performed, and also, mechanical fatigue testing with a higher number of cycles should be done.

CONCLUSION

Considering the limitations of this laboratory experiment, the results showed the following: In case

of single restorations, the internal connections were more stable than external connections, and the Morse taper connection showed a better stability than the internal hexagon and external hexagon connections after mechanical cycling.

CLINICAL CONCLUSION

When properly indicated, the Morse taper connection may exhibit improved stability of the prosthesis even after mechanical stress.

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